

1 **Movement Regularity Differentiates Specialized and Non-Specialized Athletes in a Virtual**
2 **Reality Soccer Header Task**

3 Christopher Riehm^{1,2,3}, Scott Bonnette⁴, Michael A. Riley⁵, Jed Diekfuss^{1,2,3}, Christopher
4 DiCesare⁶, Andrew Schille^{1,2,3}, Adam W. Kiefer⁷, Neeru A. Jayanthi^{1,2,3}, Stephanie Kliethermes⁸,
5 Rhodri S. Lloyd⁹, Mathew W. Pombo^{1,2,3}, Gregory D. Myer^{1,2,3,10}

6 ¹Emory Sports Performance And Research Center (SPARC), Flowery Branch, GA, USA

7 ²Emory Sports Medicine Center, Atlanta, GA, USA

8 ³Department of Orthopaedics, Emory University School of Medicine, Atlanta, GA, USA

9 ⁴Division of Sports Medicine, Cincinnati Children's Hospital Medical Center, Cincinnati, Ohio, USA

10 ⁵Department of Rehabilitation, Exercise, & Nutrition Sciences, University of Cincinnati

11 ⁶Department of Mechanical Engineering, University of Michigan, Ann Arbor, MI, USA

12 ⁷Department of Exercise and Sport Science, University of North Carolina at Chapel Hill, Chapel Hill,
13 USA

14 ⁸Department of Orthopedics and Rehabilitation, University of Wisconsin-Madison, Madison, WI,
15 USA

16 ⁹School of Sport and Health Sciences, Cardiff Metropolitan University, Cardiff, United Kingdom

17 ¹⁰The Micheli Center for Sports Injury Prevention, Waltham, USA

18
19 **Corresponding Author:**

20 Christopher Riehm, PhD.

21 Email: criehm@emory.edu

22 Phone: 4109673378

23
24 **Funding Source:**

25 NIH: 1U01AR067997-01A1

26
27 **Take Home Points:**

- 28 1) Specialized and non-specialized athletes exhibit different degrees of movement
29 regularity when assessed in a sport specific virtual reality environment.
30 2) The sport specific virtual reality assessment exposed group differences in body
31 movement regularity that were not seen on the DVJ assessment.
32
33
34
35

36 **Movement Regularity Differentiates Specialized and Non-Specialized Athletes in a Virtual**
37 **Reality Soccer Header Task**

38

39 **Abstract**

40 Young athletes who specialize early in a single sport may subsequently be at increased risk of
41 injury. While heightened injury risk has been theorized to be related to volume or length of
42 exposure to a single sport, the development of unhealthy, homogenous movement patterns and
43 rigid neuromuscular control strategies may also be indicted. Unfortunately, traditional laboratory
44 assessments have limited capability to expose such deficits due to the simplistic and constrained
45 nature of laboratory measurement techniques and analyses. To overcome limitations of prior
46 studies, we proposed a soccer-specific virtual reality (VR) header assessment to characterize the
47 generalized movement regularity of 44 young female athletes relative to their degree of sport
48 specialization (high versus low). Participants also completed a traditional drop vertical jump
49 (DVJ) assessment. During the VR header assessment, significant differences in center of gravity
50 sample entropy (a measure of movement regularity) were present between specialized [Center of
51 Gravity (COG) SampEn: $M = .08$, $SD = .02$] and non-specialized (COG SampEn: $M = .10$, $SD =$
52 $.03$) groups. Specifically, specialized athletes exhibited more regular movement patterns during
53 the soccer header than the non-specialized athletes. However, no significant between-group
54 differences were observed when comparing participants' COG time series data from the drop
55 vertical jump assessment. This pattern of altered movement strategy indicate that realistic, sport-
56 specific VR assessments may be uniquely beneficial in exposing overly rigid movement patterns
57 of individuals who engage in repeated sport specialized practice.

58 **Keywords:** Sample Entropy, Complexity, VR

59 Introduction

60 In recent years, young athletes increasingly participate in a single sport for a significant
61 portion of each year and refrain from participating in other sports.¹ This increase in sport
62 specialization may be driven by coaches, parents, and peers who encourage early, specialized
63 practice to enable the achievement of elite performance.² However, a systematic review
64 concluded that sport specialization does not result in improved task or career performance
65 compared to non-specialized peers.³ Many sports, in fact, may allow for intensive, sport-specific
66 training to begin much later in adolescence without detrimental consequences on performance.⁴
67 Furthermore, there are major concerns that early specialization contributes to increased rates of
68 overuse injury in young athletes.⁵

69 Although precise injury mechanisms remain unknown, researchers hypothesize that
70 immature athletes are less equipped than mature or adult athletes to accommodate repetitive
71 stresses to musculoskeletal tissue.⁶ Specialization in a single sport may increase exposure to
72 repetitive stresses that amplifies the risk of injury to the joints and tissue under repetitive load
73 (e.g., baseball pitching and injuries to the elbow and shoulder⁷). Emerging evidence also
74 demonstrates that early sport specialization may introduce maladaptive biomechanical
75 differences between specialized and non-specialized athletes, particularly during maturation.⁸
76 Additionally, highly specialized young athletes are more likely to develop overuse injury when
77 compared to non-specialized peers.⁹ Despite this evidence, there are few objective criteria
78 available to quantify appropriate thresholds and diversification of sport participation by young
79 athletes. Therefore, to appropriately inform athletes, coaches, and parents about the risks
80 associated with sport specialization it is vital that the mechanism behind specialization-driven
81 biomechanical change is discovered.

82 One way to uncover the mechanisms that lead to injury in young athletes is by analyzing
83 the variability of their sport-relevant movement patterns. Movement variability measures capture
84 how an athlete's body moves over time and can offer a detailed picture of athletic performance
85 and potential injury mechanisms. For example, it is not only important to know how many
86 pitches a baseball pitcher throws for a 'strike' or how fast they throw the ball, but also how the
87 form of their pitching movement varies between pitches. Some pitchers may change their
88 movements very little from pitch to pitch, exhibiting highly regular movement patterns, while
89 others may throw differently on every pitch, a more irregular pattern. While irregular movements
90 may be negatively viewed as reflecting inconsistency, they may also represent the offloading of
91 repeated stress onto a larger set of tissues. Moreover, different styles of movement variability
92 result from an athlete's response to evolving circumstances during play and therefore
93 characterizing movement variability may provide valuable insight into the perceptual-motor
94 strategies that athletes use to accomplish their on-field goals.

95 Movement variability measures are uniquely suited for sports biomechanics analysis due
96 to the ubiquity of high-quality time-series data produced by widely used optical motion capture
97 systems. Analyses of movement variability, however, have often been overlooked in favor of
98 discrete biomechanical and performance measurements such as peak joint angles and moments,¹⁰
99 with many researchers viewing movement variability as noise or error rather than as an intrinsic
100 feature of a properly functioning system.¹¹ Although not widely studied in the context of sport
101 specialization, specific patterns of movement variability have been linked to overuse injury.¹²
102 Healthy movement systems exhibit a characteristic mode of variability, which allows the system
103 to overcome unexpected perturbations and adapt to changing circumstances¹³ while distributing
104 forces experienced during activity across a variety of structural tissues. Sample entropy

105 (SampEn) is one nonlinear time-series analysis that has been used successfully to quantify the
106 structure of movement variability, with smaller values of SampEn corresponding to a greater
107 degree of regularity (e.g., a sine function) and larger values corresponding to more irregularity
108 (e.g., white noise). To date, SampEn has been used extensively in movement science and sport
109 science to study posture and balance¹⁴⁻¹⁶, sensorimotor control¹⁷, stroke¹⁸, and concussion.^{19,20}
110 SampEn has also provided insight into the dynamics of human gait²¹ as well as overall team
111 sport performance.²²

112 To complement nonlinear analytic techniques, testing environments should also be
113 appropriately dynamic to isolate differences in movement variability that generalize to actual
114 sport. Immersive virtual reality (VR) is one method that enhances testing by offering an
115 experience that mimics on-field play in a controlled environment that can easily be combined
116 with a laboratory-based motion capture system. Unlike on-field motion-capture solutions,
117 laboratory-based motion capture can be standardized using VR and allow the experimenter to
118 precisely control the perceptual information that is delivered to an athlete. Further, VR offers a
119 significant enhancement to traditional laboratory assessments, which may be too simplistic to
120 elicit the sort of perceptual-motor behavior that characterizes an athlete's on-field play.^{23,24}
121 Often, laboratory assessments lack the features of the sport-specific contexts, such as dynamic
122 opponents and objects (balls, goals, etc.), that may drive the movement patterns of athletes.²⁵
123 This may be especially true if the athletes have varying degrees of specialization in a particular
124 sport. For instance, a highly specialized soccer athlete may develop unique, possibly detrimental
125 movement patterns in the context of a soccer game that are not expressed during general
126 laboratory assessments. Therefore, a meaningful comparison with non-specialized athletes would
127 require a soccer-specific context. Although not in widespread usage, VR is gaining traction as a

128 useful tool in sports training and assessment²⁶ and has previously been used to characterize the
129 throwing kinematics of handball players,²⁷ to identify anterior cruciate ligament (ACL) injury
130 risk profiles,²⁸ and enhance knee biomechanics after ACL reconstruction.²⁹

131 One notable utilization of VR related to musculoskeletal injury risk was a prior report
132 using a soccer-specific header scenario to identify high-risk lower extremity biomechanics in
133 adolescent athletes.²⁵ This work identified biomechanical deficits associated with ACL injury
134 that were magnified during the sport-specific VR task when compared to a drop vertical jump
135 (DVJ) task, indicating the possibility that sport-specific VR may be a more sensitive testing
136 method. While simple landing tasks such as the DVJ have been informative about the
137 biomechanics of injury risk,³⁰ they do not provide the same degree of realism as the sport-
138 specific VR header scenario. While both require a single jump as their main feature, the soccer
139 header scenario is more dynamic and requires continuous sensorimotor coordination of the entire
140 body with “external” virtual objects and stimuli, namely the incoming soccer ball, goalie, and
141 goal. Examining whole-body movement strategies is especially relevant in the context of lower
142 extremity injury (e.g., of the ACL),³¹ given the apparent links between upper and lower body
143 mechanics that give rise to deficits underlying injury.³² The DVJ, on the other hand, is more
144 rigidly structured and requires that the athlete follow formal instructions and perform a relatively
145 simplistic movement. In this study, we aimed to leverage the realism of the previously used VR
146 header scenario to explore movement patterns of specialized and non-specialized athletes.

147 Although heading the ball in soccer is performed infrequently relative to other movements
148 (running, cutting, etc.), significant injuries do occur during this complex task and warrant
149 investigation. Further, we chose the header task here because it requires the athlete to perform a
150 difficult visual coordination task (reflecting the ball off their head and into the goal) in mid-air,

151 while simultaneously requiring an athlete to maintain safe lower extremity alignment with
152 restricted sensorimotor resources (attention diverted towards the incoming ball and away from
153 landing mechanics). The VR header thus naturally extends the demands of the drop vertical jump
154 (i.e., motor control/landing biomechanics) by sharing important classification features (a task
155 that exposes sensitive and specific injury risk factors) and increasing demands on the
156 sensorimotor system (additive neurocognitive constraints). Previous work has compared soccer
157 specific jumping with the DVJ and found them to be significantly different in the precise
158 mechanics used by the athlete.³³ We look to build upon this by improving the realism of the
159 soccer specific jumping condition, namely by employing virtual reality to simulate realistic ball
160 trajectories, requiring movements that are highly similar those performed on-field.

161 The primary purpose of the current investigation was to evaluate differences in
162 movement variability between specialized and non-specialized athletes using both sport-specific
163 VR and traditional landing tasks. We hypothesized that differences in movement variability,
164 indexed by SampEn, would be present during the soccer-specific VR scenario between
165 specialized and non-specialized athletes, but between-group differences would be less apparent
166 during a traditional laboratory assessment of injury risk (DVJ).

167 **Method**

168 *Participants*

169 A total of 91 female adolescent soccer athletes participated in this investigation. While no
170 a priori analysis was performed, prior VR work using 3D motion analysis found significant
171 between-group differences with a total enrolment of 38 individuals, so we enrolled a greater
172 number of participants to exceed the sample size of this prior publication²⁸ to account for the

173 subsequent categorization and final analyses that would be grouped by sports specialization
174 (~three times larger initial n in present work). Our participants represented a subgrouping of
175 participants in a larger neuromuscular training study of soccer, basketball, and volleyball
176 athletes. The current investigation includes data collected from soccer athletes during baseline
177 testing periods, which preceded neuromuscular training exposures. All participants reported no
178 recent injury or any physical or neurological condition that would preclude them from
179 participating in sports. All participants and their legal guardians provided informed, written
180 consent/assent before the start of the investigation. Institutional review board approval was
181 obtained prior to the initiation of the investigation.

182 *Sports Participation Questionnaire*

183 To classify the degree of specialization of each participant, they were asked, prior to
184 participation, to complete a short sport-specialization questionnaire that has been used in
185 previous work to index an athletes degree of specialization.⁹ The questionnaire consisted of the
186 following 3 ‘yes’ or ‘no’ questions: “Could you pick a main sport that you participate in?”; “Did
187 you quit other sports to focus on a main sport?”; “Do you train for a single sport greater than or
188 equal to 8 months a year?”. The number of “yes” answers was tallied such that each participant
189 was assigned a score from 0 to 3. Participants receiving a 0 or 1 were placed in the non-
190 specialized group and those who received a 3 were placed in the specialized group. Participants
191 receiving a score of 2 were considered moderately specialized.

192 The final breakdown by specialization group was fourteen athletes (32%) in the non-
193 specialized group (age: $M = 14.68$, $SD = 1.2$) and thirty athletes (68%) in the specialized group
194 (age: $M = 15.04$, $SD = 0.53$). Preliminary statistical analysis confirmed non-significant age,
195 height, and weight differences between specialization groups.

196 *Motion capture data collection*

197 During their participation in this study, participants were outfitted with infrared reflective
198 markers and their motions were recorded using a 22 (DVJ) or 44 (VR) camera motion capture
199 system (Raptor-E, Motion Analysis, Santa Rosa, CA, USA) sampled at 240 Hz. A minimum of
200 three markers were placed on each body segment in a non-collinear arrangement. Landmarks on
201 the participant's anatomy and VR equipment included: four attached to the head (via the head
202 mounted display), sternum, sacrum, offset, and bilaterally on the acromioclavicular joints,
203 elbows, mid-wrists, medial and lateral hands, anterior superior iliac spine, greater trochanters,
204 mid-thighs, medial and lateral femoral condyles, tibial tuberosities, lateral shanks, distal shanks,
205 medial and lateral malleoli, heels, toes, lateral foot, and posterior foot. Participants wore a
206 standardized shoe (Supernova Glide 2, Adidas, Herzogenaurach, Germany), within which the
207 foot markers were embedded.

208 *Procedure*

209 Prior to participation in the virtual header task, participants completed DVJ test. For the
210 DVJ, participants were instructed to hop from a 12-inch box, land and then immediately jump to
211 grab a basketball, which was suspended at their previously determined maximum jump height.
212 Prior to performing the DVJ, all participants saw a demonstration of proper DVJ form by one of
213 the experimenters. Importantly, the experimenter demonstrated that both feet should leave the
214 box simultaneously and land without shifting. Any participant's trials that did not follow this
215 form were repeated, with corrective instructions until three successful trials were completed.

216 Next, participants completed the virtual soccer task as previously reported.²⁵ First, they
217 were outfitted with a Vive Pro virtual reality headset (HTC, Taoyuan City, Taiwan) through

218 which they viewed the virtual reality environment and a virtual avatar of themselves, from the
219 first-person perspective (*Figure 1a*). Immediately after putting on the headset, participants
220 underwent a self-paced familiarization session (5-7 minutes in total) consisting of walking,
221 jogging, and running within the boundaries of the virtual space, meant to acclimate the
222 participants to moving freely in VR while also introducing them to the layout and safety features
223 of the VR environment. Prior work has used a similar familiarization session to effectively
224 acclimate athletes to a virtual environment.²⁸ During this session, participants were shown the
225 boundaries of the virtual space (*Figure 1b*), which would become visible if the participant moved
226 outside of the central area of the motion capture space. After the familiarization session,
227 participants were provided with automated audio-visual instructions which introduced the VR
228 soccer header scenario. For the header scenario, a virtual, animated character, located at either
229 the right or left corner of the soccer field, would perform a corner kick aimed towards a spot just
230 outside the penalty box in the center of the field. For each kick, the participant was required to
231 run from a starting position (labeled in *Figure 1b*) and then jump and attempt to head the virtual
232 ball into the goal. The participant saw a total of 6 corner kicks, 3 from each side of the field,
233 including one practice trial for each side. The side from which the ball was kicked was randomly
234 selected in a trial-by-trial fashion. The duration of each trial was identical for all participants.
235 Participants were instructed to time their jump to land on the spotlight, which was visible on the
236 grass in front of the goal (*Figure 1 (a and b)*). During the header scenario, two experimenters
237 monitored each participant. One experimenter operated the VR scenario from a computer
238 workstation and could see everything that each participant could see while the other
239 experimenter stayed in the open floor area with the participant to give verbal guidance if needed
240 and ensure that participants were always safe. If participants performed the header in an

241 obviously wrong manner (e.g. did not jump or cut in the wrong direction), one of the
 242 experimenters would provide verbal corrections.

243 *Data Clean Up and Sample Entropy Analysis*

244 After data collection, all motion capture data was tracked and quality controlled to
 245 remove artifacts and spurious data and then post-processed using Visual3D (C-Motion Inc,
 246 Germantown, MD, USA). Marker trajectories were filtered using a 4th order low-pass
 247 Butterworth filter with a cutoff frequency of 12 Hz, and a 12-segment, 6-degree-of-freedom
 248 model was applied to the marker trajectories to compute each tracked segment's position and
 249 orientation at each time sample. The model was scaled to each participant's weight and height,
 250 and the vertical (Z axis) center of gravity (COG) time series for each DVJ and VR trial was
 251 computed as:

$$252 \quad \text{COG} = \frac{\sum_{i=1}^{12} m_i r_i}{M}$$

253 where m_i and r_i were the mass and vertical position of the i th segment, respectively, and M was
 254 the total body mass.

255 The COG time series was chosen for SampEn analysis because it exhibits a general
 256 profile of movement variability during the header task. Applying SampEn analysis to the COG
 257 trajectory is an effective way of indexing the global dynamics of whole-body motor
 258 coordination. Each COG time series spanned the duration of a given DVJ or VR trial. All COG
 259 trajectories from the 44 participants with complete data were subsequently submitted to
 260 SampeEn analysis yielding a single value of SampEn per trial and per participant. SampEn
 261 values for each trial were then averaged to produce a single SampEn value per participant and
 262 per task. All SampEn values were calculated using a radius value of .01 and an embedding

263 dimension of 1. These parameters were estimated following the procedure outlined by Ramdani
264 et al.¹⁷ For this data, which is largely comprised of ballistic jumping movements, we initially
265 tested larger radius values, but found that the analysis became oversaturated with template
266 matches, resulting in a floor effect where all trajectories produced extremely low values of
267 sample entropy. Although Ramdani et al. do not explicitly test or recommend radius values as
268 low as .01 for quiet-stance postural COP data, there is no recommendation given for ballistic
269 movements of the sort that we tested. For our data, the radius value represented between 10 and
270 15% of the standard deviation of each time series. Data were not normalized to retain the full
271 profile of the jumping movement. For our analysis, the radius value of .01 equates to a real
272 distance of 10 millimeters, which is well above the measurement precision of the motion capture
273 system.

274 **Statistical Approach**

275 The intent of this study was to compare the regularity of movement variability of specialized and
276 non-specialized athletes on two tasks (VR header and DVJ). Therefore, average vertical COG
277 SampEn values for the DVJ and VR header tasks were submitted separately to independent
278 sample *t*-tests with sport specialization (specialized, non-specialized) as the between group
279 factor. Alpha was set *a priori* at $p < .05$ to determine statistical significance. Cohen's *D* effect
280 sizes were also reported to support interpretation of the magnitude of between group differences.
281 To ensure the integrity of these results, groups were tested for outliers, normality, and
282 homoskedasticity. No significant abnormalities were identified.

283 **Results**

284 Participant removals were done prior to analysis due to age, specialization, and
285 incomplete data (see *Figure 2*). First, data from nine participants were found to be incomplete.
286 Incomplete data resulted from missing markers that prevented reliable calculation of the COG
287 and could not be recovered with post processing methods. For the purposes of the current
288 investigation, participants were placed in non-specialized, moderately specialized, and
289 specialized groups based on the sports participation questionnaire, described above. Participants
290 who were categorized as moderately specialized were not included in the current investigation,
291 leaving 69 participants remaining. Furthermore, due to a drastic inequality of 16- and 17-year-
292 old athletes in the high (15 individuals) and low (1 individual) specialization groups, the decision
293 was made to remove all 16- and 17-year-old athletes from the current analysis. Due to the
294 exclusions based on sport specialization status, age, and incomplete motion capture data a final
295 grouping of forty-four female soccer athletes was included in the current analysis.

296 For the VR soccer header task, a significant difference in COG SampEn was found
297 between non-specialized (COG SampEn: $M = .10$, $SD = .03$) and specialized groups (COG
298 SampEn: $M = .08$, $SD = .02$), $t(42) = 2.54$, $p = .015$ $d = .82$. Sample header COG trajectories
299 with high and low relative SampEn are presented in *Figure 3*, showing an example of the greater
300 regularity of body movement observed in specialized athletes compared to non-specialized
301 athletes.

302 COG SampEn values for DVJ trajectories, averaged per individual, were also compared
303 between the non-specialized (COG SampEn: $M = .021$, $SD = .004$) and specialized (COG
304 SampEn: $M = .022$, $SD = .003$) groups, and no significant differences were found $t(42) = 1.26$, p
305 $= .21$ $d = .41$. *Figure 4* shows 3 example COG trajectories from one participant performing the
306 DVJ, which are noticeably less complex than even the low complexity example in *Figure 3*. This

307 is also reflected in the lower mean sample entropy values from both groups on the DVJ than the
308 same groups on the header task.

309 **Discussion**

310 The primary purpose of this project was to investigate differences in the regularity of
311 movement variability between specialized and non-specialized athletes during a sport-specific VR
312 jump-landing (soccer header) task and a traditional injury risk assessment laboratory task (DVJ).
313 As hypothesized, specialized and non-specialized athletes demonstrated differences in movement
314 regularity (i.e. COG SampEn) during the soccer-specific header task, but no similar significant
315 differences were identified for the DVJ. The directionality of SampEn differences indicate that
316 non-specialized athletes exhibited less regular movement patterns during the VR soccer header
317 than the specialized athletes. These results also indicate that using VR to engage athletes in similar
318 sensorimotor circumstances to those which take place during real play can provide crucial insights
319 into possible injury mechanisms, which are unavailable using traditional lab-based biomechanical
320 measurements.

321 The current results show that the body movement of specialized athletes is more regular
322 during a realistic soccer header task than the movement of non-specialized athletes. Our
323 interpretation of this is grounded in the notion that sport specific practice of movements such as
324 the header establish “hard wired” movement patterns that persist and solidify if the athlete does
325 not frequently practice movements of a different sort. While “hard wired” movements may allow
326 the athlete to perform well in drills and possibly even in games, it is also possible that this reduced
327 variability, compared to the non-specialized athletes, over time, would lead to a higher likelihood
328 of overuse injury due to more homogenized muscle activation patterns.³⁴ Athletes who play
329 multiple sports and participate in a larger variety of drills and on-field scenarios could potentially

330 reduce their risk of overuse injury by offloading the stress and strain of their movements onto more
331 muscles and connective tissues. This hypothesis, however, cannot be confirmed with the current
332 data as no overuse injuries have been reported for the set of athletes who participated in this study.
333 Once this linkage is better understood, we would recommend that biomechanical training
334 interventions to address these deficits be implemented to reduce overuse injury risk. Additionally,
335 within-sport changes to drilling and coaching could reduce the regularity of movement patterns
336 without the need for athletes to take on the responsibility of playing multiple sports. Importantly,
337 these changes to athletic practice apply not only to healthy athletes, but also those who are
338 undergoing rehabilitation. It is vital that these athletes' re-structure their movement patterns during
339 the process of rehabilitation so that they can return to sport with renewed injury resistance.

340 Beyond overuse injury risk, the difference in movement regularity between specialization
341 groups may be indicative of differential sensorimotor adaptability. Specifically, differences in
342 movement regularity could render specialized and non-specialized differently able to respond to
343 unexpected perturbations that arise during the performance of a soccer header. Theoretical support
344 for this view can be found in the theory of Optimal Movement Variability.³⁵ This view posits an
345 optimal range of movement variability for a given activity, within which athletes can accommodate
346 disruptions to their activity (e.g. redirection of a ball during a soccer header) without injury.
347 Notably, movement regularity that is both greater and less than the bounds of this optimal range
348 may increase susceptibility to injury. For the current results it is difficult to say, without further
349 experimentation, where this optimal range lies and if the movement variability of non-specialized
350 and specialized athletes is optimal and sub-optimal, respectively. However, the presence of a
351 difference at all indicates that this is a question that requires additional investigation. The current
352 results also show that such future investigations should be carried out using realistic sport-specific

353 VR tasks to complement traditional laboratory assessments, such as the DVJ. The DVJ and similar
354 assessments may not be ideal as they don't allow athletes to move with the same variety that they
355 would on the field and so they may not elicit the style of movement regularity that would
356 characterize their real in-game behavior. As can be seen when inspecting the movements made
357 during the DVJ (*Figure 4*), this task elicits an almost purely sinusoidal COG movement in the
358 vertical dimension, the regularity of which does not vary meaningfully between groups. Our
359 contention is that this largely reflects the highly restrictive nature of the DVJ task, which may
360 meaningfully suppress any individual- or group-specific characteristics of the tested athletes'
361 movement. Contrasted to the DVJ, the sport specific VR header task was much more free-form
362 and allowed the athlete to naturally interpret the task, therefore generating an overall set of
363 movement trajectories that is more representative of the range of dynamics that should be expected
364 from the population that our sample was derived from (female youth soccer athletes). Inspection
365 of *Figure 3* clearly differentiates the VR movements from those of the DVJ. The trajectories from
366 the VR header suggest that the nature of the lead-up to the required jump are an important factor
367 driving the regularity of the athletes' movements. Athletes were only required to cover the distance
368 between a starting point and the location where they met the ball, leaving an appreciable period
369 within which athletes could move in a naturalistic fashion. It is our belief that this provides a
370 window onto an athlete's on-field behavior that has been unavailable to more formalized
371 biomechanical tests (i.e. the DVJ).

372 Future work may seek to expand on the current finding by probing deeper into the
373 neuromuscular and task organization of sport-specific tasks like the soccer header studied here.
374 While the soccer-specific header scenario used in this investigation provided a realistic context for
375 the athlete, it was not used to directly manipulate the sensory-motor coordination underlying the

376 performance of a header to better understand the underlying mechanism. Additionally, it would
377 also be important to evaluate possible coordination deficits in specialized athletes through peak
378 height velocity and skeletally mature athletes to determine if specialization or stage of
379 development is a bigger risk. Future work could investigate, also, if visual perception (i.e., as it
380 relates to coordination with the ball) during a header task plays an important role in causing
381 differential behavior of specialized and non-specialized athletes' neuromuscular systems. Such
382 work would be uniquely empowered by comprehensive control over an athlete's visual
383 environment that is provided by VR. Along these lines, work using dynamic stroboscopic feedback
384 disruption has been used to differentiate the visuo-motor control strategies of those who underwent
385 ACL reconstruction from matched controls^{36,37}, demonstrating the essential role of visuomotor
386 control in driving healthy landing biomechanics.

387 Another interesting direction for future research would be to investigate the specific
388 neurological factors that drive differences in sensory-motor function between specialized and non-
389 specialized athletes. While the differences in gross body movement complexity found in this study
390 are a promising indicator that specialization is associated with distinctive sensory-motor control
391 strategies, there is still much to be uncovered at the neurological level. Future work could seek to
392 understand the neurological basis of the different movement patterns uncovered in this
393 investigation by applying neuroimaging techniques to specialized and non-specialized athletes.
394 Previous work has identified divergent electrocortical dynamics in individuals who demonstrate
395 injury-prone biomechanics.³⁸ A similar approach could very well identify distinct neurological
396 factors which support movement pattern complexity differences that result from specialized
397 training. Specifically, future work may be warranted to investigate the relationship between an
398 athlete's history of concussion and their movement variability. Concussion is a widespread and

399 deeply impactful sports injury with a long-term impact on an athletes quality of life as well as their
400 risk for future musculoskeletal injuries and could possibly have contributed to the current results,
401 although this was not explicitly measured.³⁹

402 One limitation to the current investigation is the lack of performance metrics to quantify
403 the focus and perception of the athlete on the corner kick. Although 3D motion capture was
404 performed for the duration of the task, no concurrent information about the position of the soccer
405 ball, or the success or failure of the goal scoring attempt were recorded. This makes it difficult to
406 qualify complexity in task or goal relevant terms, which some have argued is critical in interpreting
407 complex movements.⁴⁰ Future work could solve this problem by synchronously recording features
408 of the virtual task (ball position, goals scored etc.) alongside the 3d motion capture. An additional
409 limitation of this study was the inequality in number of athletes per group (specialized vs non-
410 specialized). Future studies that focus on youth sport specialization should balance recruitment
411 such that participating athletes fall equally in the specialized and non-specialized groups.

412 One key consideration that can be drawn from the current work is the potential to utilize
413 virtual reality training to improve movement variability adjunctively to on-field training. In
414 addition, for athletes undergoing rehabilitation or younger athletes who are developing
415 neuromuscular control, virtual reality may be a safe alternative to scenarios associated with
416 undesirable head impact exposure, including physical contact with the ball (e.g. headers) and/or
417 other players. Although head impacts sustained during practice are often sub-concussive, there is
418 still significant concern for the negative long-term effects resultant from repetitive exposure.⁴¹
419 While one could simply limit head impact exposure by limiting time spent playing, that would
420 deprive athletes from the sensorimotor experience that leads to injury-resistance and the physical
421 practice necessary to achieve desired performance outcomes. In this light, immersive virtual reality

422 such as that used in the current investigation, could offer the opportunity to enhance movement
423 strategies related to sport-specific movements without the undesirable risks associated with high
424 head impact exposure. To this end, virtual reality equipment and software has drastically improved
425 its availability to individual consumers, as well as to clinicians looking to improve their patient's
426 readiness for sport. Current state of the art virtual reality systems can be purchased for a few
427 hundred dollars with a range of software options available for sports specific and generalized
428 training programs that address sensorimotor acuity, cognitive skills, and overall fitness. Based on
429 the current results there is potential to employ virtual reality training strategies to augment
430 traditional training methods, especially for those who are not physically prepared or rehabilitated
431 to a point that they would be safe to be exposed to full contact sports

432 **Conclusion**

433 The current work investigated the regularity of movement patterns from young athletes
434 performing both a realistic VR soccer header task and a standard DVJ assessment. The purpose
435 of this work was to determine if specialized and non-specialized athletes exhibited differences in
436 movement regularity during performance of those tasks. The results confirmed that the COG
437 trajectories of specialized and non-specialized athletes differed with respect to movement
438 variability as assessed by the SampEn metric. This pattern of results indicates that realistic,
439 sport-specific VR assessments may be uniquely beneficial to expose overly rigid movement
440 patterns of individuals who engage in repeated sport specialized practice. Further, since only the
441 VR task was able to expose these movement differences in athletes, future considerations are
442 warranted relative to standardized laboratory tasks and possibly the need for enhanced ecological
443 validity in athlete assessments of injury risk. Training programs and rehabilitation, also, should
444 include tools and techniques that maximize the variety and realism of athletic movements. Where

445 possible newly affordable and accessible VR technology should be applied to ensure that at-risk
446 and developing athletes are able to manage the dangers of physical contact while continuing to
447 develop sport-related sensorimotor skills.

448

449

450

451

452

453

454

455

456

457

458

459

460

461

462

463

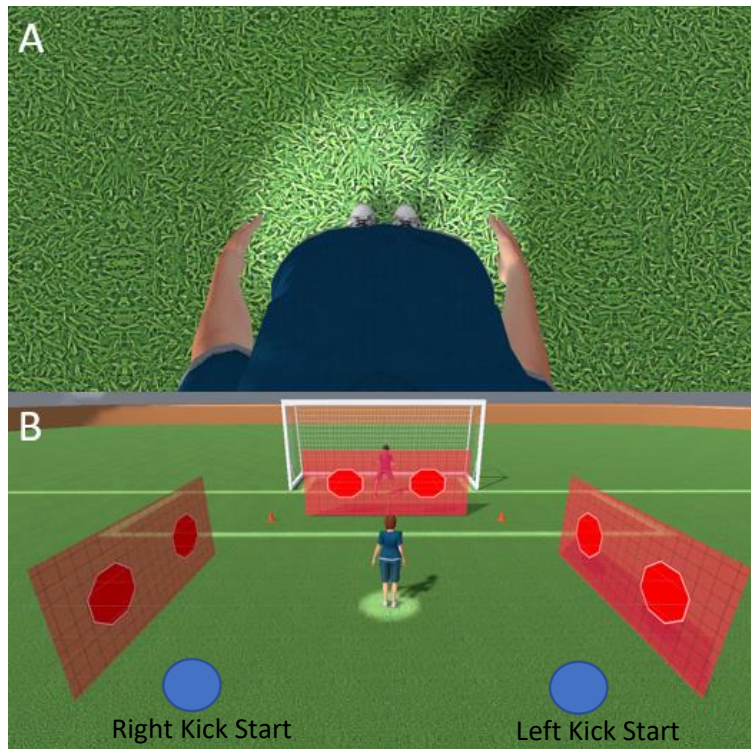
464 **References**

- 465 1. Bell DR, Post EG, Trigsted SM, Hetzel S, McGuine TA, Brooks MA. Prevalence of sport
466 specialization in high school athletics: a 1-year observational study. *The American Journal of Sports*
467 *Medicine*. 2016;44(6):1469-1474.
- 468 2. Baxter-Jones ADG, Maffulli N. Parental influence on sport participation in elite young athletes.
469 *Journal of Sports Medicine and Physical Fitness*. 2003;43(2):250-255.
- 470 3. Jayanthi N, Kliethermes SA, Côté J. Youth sport specialisation: the need for an evidence-based
471 definition. BMJ Publishing Group Ltd and British Association of Sport and Exercise Medicine; 2020.
- 472 4. DiFiori JP, Quidici C, Gray A, Kimlin EJ, Baker R. Early single sport specialization in a high-
473 achieving us athlete population: comparing National Collegiate Athletic Association student-athletes and
474 undergraduate students. *Journal of athletic training*. 2019;54(10):1050-1054.
- 475 5. Brenner JS, Medicine CoS, Fitness. Overuse injuries, overtraining, and burnout in child and
476 adolescent athletes. *Pediatrics*. 2007;119(6):1242-1245.
- 477 6. Hawkins D, Metheny J. Overuse injuries in youth sports: biomechanical considerations. *Medicine*
478 *& Science in Sports & Exercise*. 2001;33(10):1701-1707.
- 479 7. Olsen SJ, Fleisig GS, Dun S, Loftice J, Andrews JR. Risk factors for shoulder and elbow injuries in
480 adolescent baseball pitchers. *The American journal of sports medicine*. 2006;34(6):905-912.
- 481 8. DiCesare CA, Montalvo A, Barber Foss KD, et al. Lower extremity biomechanics are altered
482 across maturation in sport-specialized female adolescent athletes. *Frontiers in pediatrics*. 2019;7:268.
- 483 9. Jayanthi NA, LaBella CR, Fischer D, Pasulka J, Dugas LR. Sports-specialized intensive training and
484 the risk of injury in young athletes: a clinical case-control study. *The American journal of sports medicine*.
485 2015;43(4):794-801.
- 486 10. Bartlett R, Wheat J, Robins M. Is movement variability important for sports biomechanists?
487 *Sports biomechanics*. 2007;6(2):224-243.
- 488 11. Riley MA, Turvey MT. Variability and determinism in motor behavior. *Journal of motor behavior*.
489 2002;34(2):99-125.
- 490 12. Hamill J, Palmer C, Van Emmerik RE. Coordinative variability and overuse injury. *Sports Medicine,*
491 *Arthroscopy, Rehabilitation, Therapy & Technology*. 2012;4(1):1-9.
- 492 13. Glazier PS, Wheat JS, Pease DL, Bartlett RM. The interface of biomechanics and motor control.
493 *Movement system variability*. 2006;1:49-69.
- 494 14. Borg FG, Laxåback G. Entropy of balance-some recent results. *Journal of neuroengineering and*
495 *rehabilitation*. 2010;7(1):1-11.
- 496 15. Hansen C, Wei Q, Shieh J-S, Fourcade P, Isableu B, Majed L. Sample entropy, univariate, and
497 multivariate multi-scale entropy in comparison with classical postural sway parameters in young healthy
498 adults. *Frontiers in human neuroscience*. 2017;11:206.
- 499 16. Menayo R, Encarnación A, Gea G, Marcos P. Sample entropy-based analysis of differential and
500 traditional training effects on dynamic balance in healthy people. *Journal of Motor Behavior*.
501 2014;46(2):73-82.
- 502 17. Ramdani S, Seigle B, Lagarde J, Bouchara F, Bernard PL. On the use of sample entropy to analyze
503 human postural sway data. *Medical engineering & physics*. 2009;31(8):1023-1031.
- 504 18. Perlmutter S, Lin F, Makhsous M. Quantitative analysis of static sitting posture in chronic stroke.
505 *Gait & posture*. 2010;32(1):53-56.
- 506 19. Johnston W, O'Reilly M, Duignan C, et al. Association of Dynamic Balance with sports-related
507 concussion: A prospective cohort study. *The American journal of sports medicine*. 2019;47(1):197-205.

- 508 20. Quatman-Yates CC, Bonnette MS, Hugentobler JA, et al. Postconcussion postural sway variability
509 changes in youth: the benefit of structural variability analyses. *Pediatric physical therapy: the official*
510 *publication of the Section on Pediatrics of the American Physical Therapy Association*. 2015;27(4):316.
- 511 21. McCamley JD, Denton W, Arnold A, Raffalt PC, Yentes JM. On the calculation of sample entropy
512 using continuous and discrete human gait data. *Entropy*. 2018;20(10):764.
- 513 22. Silva P, Duarte R, Esteves P, Travassos B, Vilar L. Application of entropy measures to analysis of
514 performance in team sports. *International Journal of Performance Analysis in Sport*. 2016;16(2):753-768.
- 515 23. Wulf G, McNevin N, Shea CH. The automaticity of complex motor skill learning as a function of
516 attentional focus. *The Quarterly Journal of Experimental Psychology Section A*. 2001;54(4):1143-1154.
- 517 24. Adams K, Kiefer A, Panchuk D, Hunter A, MacPherson R, Spratford W. From the field of play to
518 the laboratory: Recreating the demands of competition with augmented reality simulated sport. *Journal*
519 *of sports sciences*. 2020;38(5):486-493.
- 520 25. DiCesare C, Kiefer A, Bonnette S, Myer G. Realistic soccer-specific virtual environment exposes
521 high-risk lower extremity biomechanics. *Journal of Sport Rehabilitation*. 2019;29:1-23.
- 522 26. Diekfuss JA, Bonnette S, Hogg JA, et al. Practical training strategies to apply neuro-mechanistic
523 motor learning principles to facilitate adaptations towards injury-resistant movement in youth. *Journal*
524 *of Science in Sport and Exercise*. 2021;3(1):3-16.
- 525 27. Bideau B, Multon F, Kulpa R, Fradet L, Arnaldi B, Delamarche P. Using virtual reality to analyze
526 links between handball thrower kinematics and goalkeeper's reactions. *Neuroscience letters*.
527 2004;372(1-2):119-122.
- 528 28. Kiefer AW, DiCesare C, Bonnette S, et al. Sport-specific virtual reality to identify profiles of
529 anterior cruciate ligament injury risk during unanticipated cutting. *IEEE*; 2017:1-8.
- 530 29. Gokeler A, Bisschop M, Myer GD, et al. Immersive virtual reality improves movement patterns in
531 patients after ACL reconstruction: implications for enhanced criteria-based return-to-sport
532 rehabilitation. *Knee Surgery, Sports Traumatology, Arthroscopy*. 2016;24(7):2280-2286.
- 533 30. Myer GD, Ford KR, Brent JL, Hewett TE. An integrated approach to change the outcome part I:
534 neuromuscular screening methods to identify high ACL injury risk athletes. *Journal of strength and*
535 *conditioning research/National Strength & Conditioning Association*. 2012;26(8):2265.
- 536 31. Zahradnik D, Jandacka D, Uchytíl J, Farana R, Hamill J. Lower extremity mechanics during landing
537 after a volleyball block as a risk factor for anterior cruciate ligament injury. *Physical Therapy in Sport*.
538 2015;16(1):53-58.
- 539 32. Zazulak BT, Hewett TE, Reeves NP, Goldberg B, Cholewicki J. Deficits in neuromuscular control of
540 the trunk predict knee injury risk: prospective biomechanical-epidemiologic study. *The American journal*
541 *of sports medicine*. 2007;35(7):1123-1130.
- 542 33. Mancini S, Dickin DC, Hankemeier D, Ashton C, Welch J, Wang H. Effects of a soccer-specific
543 vertical jump on lower extremity landing kinematics. *Sports Medicine and Health Science*. 2022;
- 544 34. Kiefer AW, Myer GD. Training the antifragile athlete: a preliminary analysis of neuromuscular
545 training effects on muscle activation dynamics. *Nonlinear dynamics, psychology, and life sciences*.
546 2015;19(4):489-510.
- 547 35. Stergiou N, Harbourne RT, Cavanaugh JT. Optimal movement variability: a new theoretical
548 perspective for neurologic physical therapy. *Journal of Neurologic Physical Therapy*. 2006;30(3):120-129.
- 549 36. Grooms DR, Chaudhari A, Page SJ, Nichols-Larsen DS, Onate JA. Visual-motor control of drop
550 landing after anterior cruciate ligament reconstruction. *Journal of athletic training*. 2018;53(5):486-496.
- 551 37. Grooms D, Appelbaum G, Onate J. Neuroplasticity following anterior cruciate ligament injury: a
552 framework for visual-motor training approaches in rehabilitation. *journal of orthopaedic & sports*
553 *physical therapy*. 2015;45(5):381-393.
- 554 38. Bonnette S, Diekfuss JA, Grooms DR, et al. Electro-cortical dynamics differentiate athletes
555 exhibiting low-and high-ACL injury risk biomechanics. *Psychophysiology*. 2020;57(4):e13530.

- 556 39. McPherson AL, Nagai T, Webster KE, Hewett TE. Musculoskeletal injury risk after sport-related
557 concussion: a systematic review and meta-analysis. *The American journal of sports medicine*.
558 2019;47(7):1754-1762.
- 559 40. Van Emmerik RE, Ducharme SW, Amado AC, Hamill J. Comparing dynamical systems concepts
560 and techniques for biomechanical analysis. *Journal of Sport and Health Science*. 2016;5(1):3-13.
- 561 41. Miller LE, Pinkerton EK, Fabian KC, et al. Characterizing head impact exposure in youth female
562 soccer with a custom-instrumented mouthpiece. *Research in Sports Medicine*. 2020;28(1):55-71.
- 563
- 564

565



566

567

568

569

570

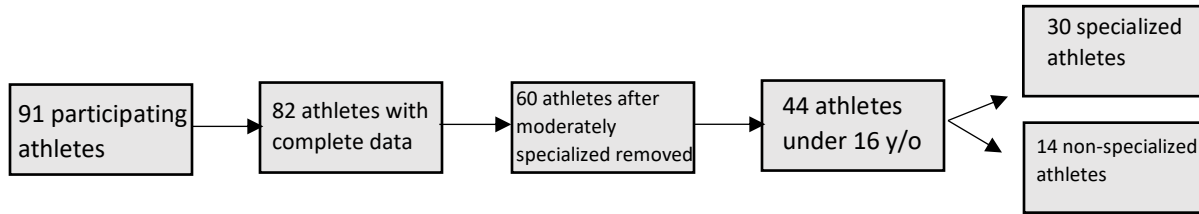
Figure 1: (a) The first person perspective of the participant's avatar and (b) the virtual boundaries that prevent a participant from approaching the laboratory walls and the starting positions for each header.

571

572

573

574



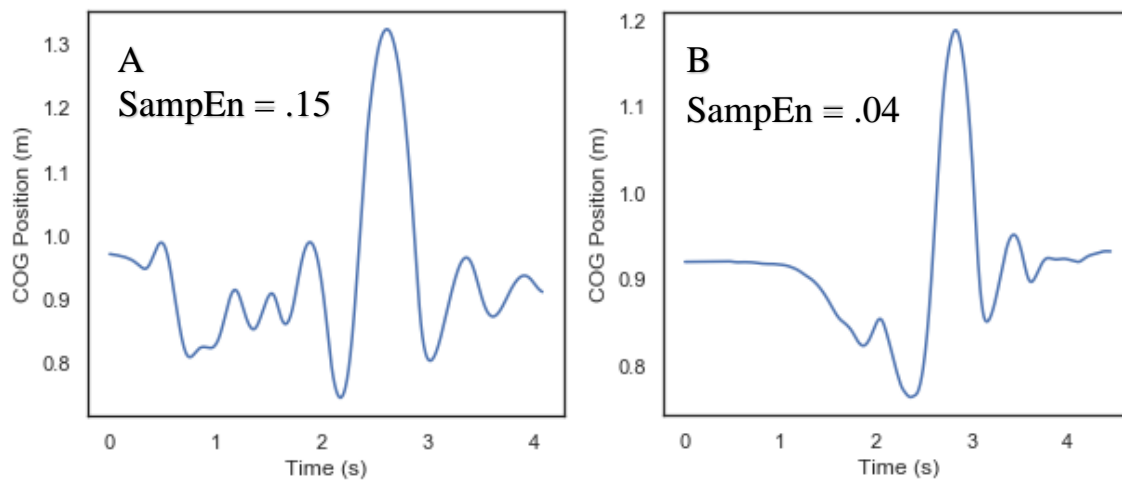
575

Figure 2: Diagram of participant removals due to incomplete data, specialization and age.

576

577

578



579

580

Figure 3: Example COG trajectories demonstrating relative high (a) and low (b) sample entropy

581

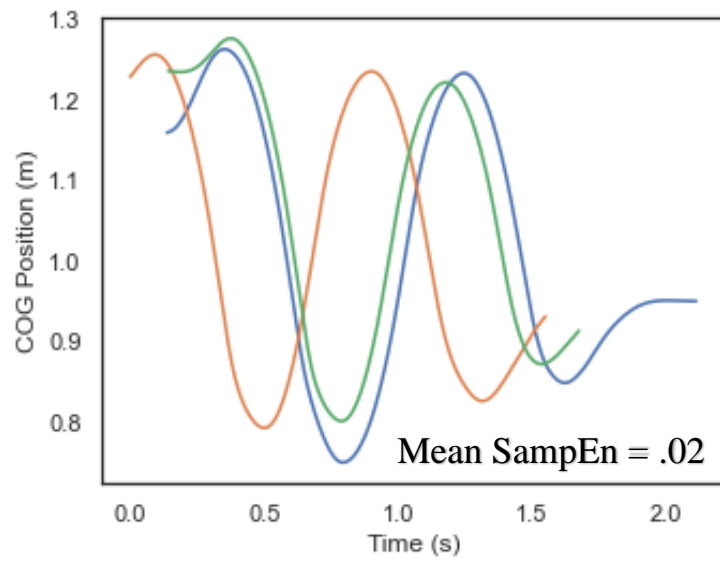
trials for the header task. These examples were drawn from non-specialized and specialized

582

individuals respectively.

583

584



585

586

Figure 4: Three example COG trajectories from a single participant's DVJ trials.

587

588